

RESEARCH ARTICLE

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ECG Patient Monitoring System Using SMTP Technology

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This paper leads to developing a Labview based ECG patient monitoring system for cardiovascular patient using Simple Mail Transfer Protocol technology. The designed device has been divided into three parts. First part is ECG amplifier circuit, built using instrumentation amplifier (AD620) followed by signal conditioning circuit with the operation amplifier (LM741). Secondly, the DAQ card is used to convert the analog signal into digital form for the further process. Furthermore, the data has been processed in Labview where the digital filter techniques have been implemented to remove the noise from the acquired signal. After processing, the algorithm was developed to calculate the heart rate and to analyze the arrhythmia condition. Finally, SMTP technology has been added in our work to make the device more communicative and much more cost-effective solution in telemedicine technology which has been key-problem to realize the diagnosis and monitoring of ECG signals. The technology also can be easily implemented over a ready existing Internet.

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I. INTRODUCTION

ECG is used to measure the rate and regularity of heartbeats, the presence of any damage to the heart, and the effects of drugs or devices used to regulate the heart (such as a pacemaker). Normally, the frequency range of ECG signals is 0.05–100 Hz and its dynamic range is 1–10 mV. The ECG signals depicted in Figure 1 is characterized by five peaks and valleys labeled by the letters P, Q, R, S, and T. The performance of ECG analyzing system depends mainly on the accurate and reliable detection of the QRS complex, as well as T- and P-waves. The P-wave represents the activation of the upper chambers of the heart, the atria, while the QRS complex and T-waves represent the excitation of the ventricles or the lower chamber of the heart. The detection of the QRS complex is the most important task in automatic ECG signal analysis. Once the QRS complex has been identified a more detailed examination of ECG signal including the heart rate and the ST segment can be performed [1,2].

Most of the modern 12-lead ECG monitoring systems are based on Einthoven's triangle, Wilson central terminal, and Goldberger augmented leads [3].

The developed ECG device is implemented on the principles of Einthoven's triangle and used lead-II configuration, as it is known as a monitoring lead, given in Figure 2.

Based on above facts, there have been numerous attempts to develop medical systems similar to the work. Such efforts are primarily led by the academia but extending deeply into the industries. However, most research efforts have been focusing on either the vital sign monitoring aspect or the ECG feature extraction using standard databases both falling short of expectation. Having analyzed the existing solutions, this work vows to bridge the two major research efforts and bring out a more realizable product to directly benefit the consumers in the medical field.

This research work offers the following contributions to the produced system; foremost is the portable ECG monitoring platform based on a 3-leads system and a design

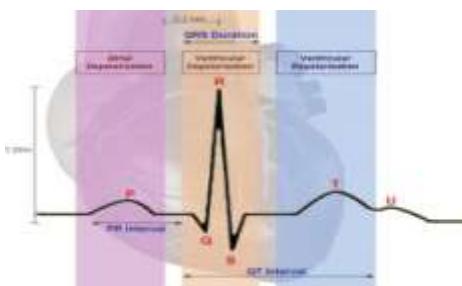
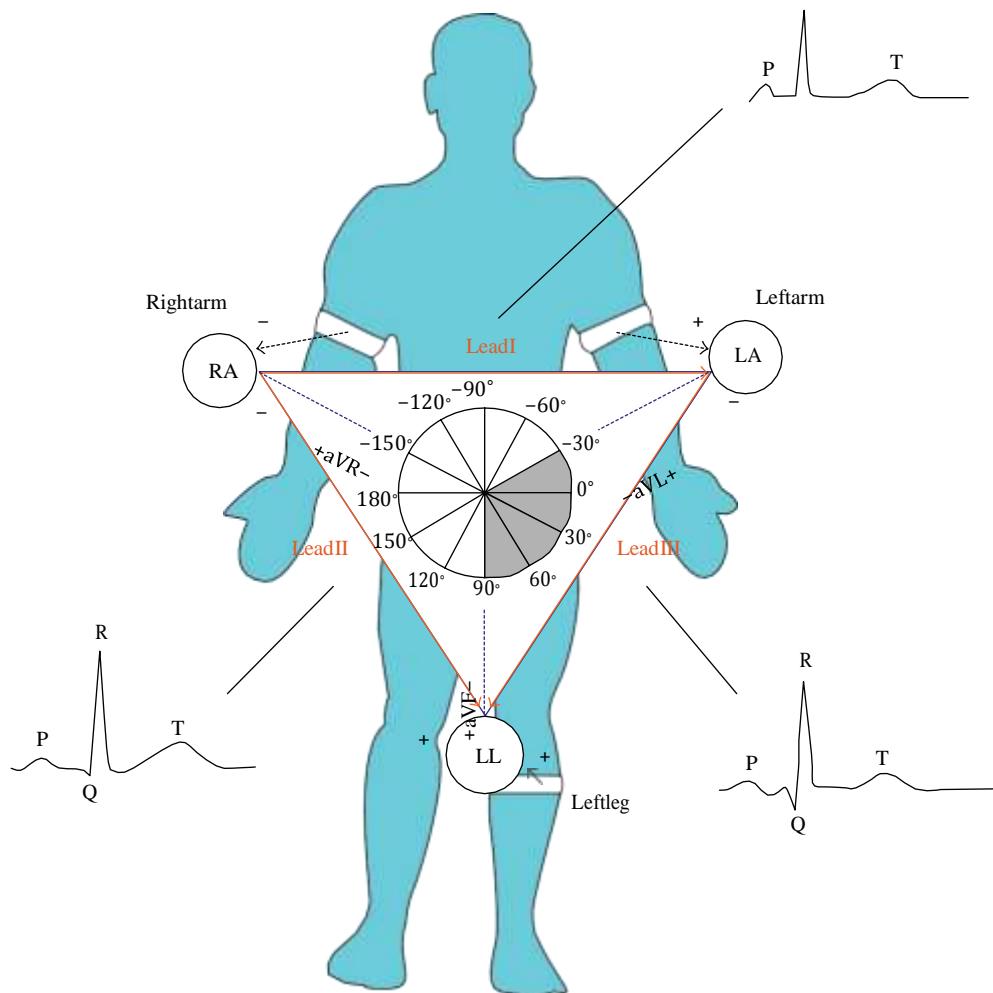


FIGURE1: Peaks of ECG.

R

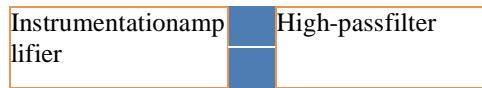


→ Bipolar limb leads

→

Augmented unipolar limb leads

FIGURE2: Electrode replacement using a 3-wire cable.



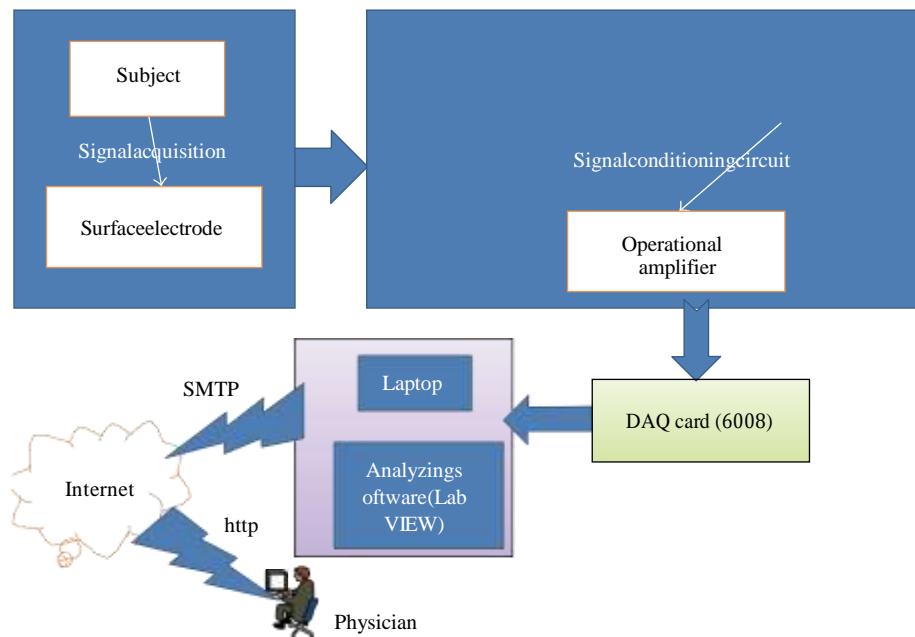


FIGURE3: BlockdiagramofproposedECGdevice.

under the NI DAQ card (6008). The ECG data was collected through the DAQ card to the PC/laptop and then transmitted to the end user (physician) through SMTP to analyze the patient condition.

Material and Method

The block diagram of the complete system is given in Figure 3. The complete design was divided into two parts: hardware and software. The hardware part comprises instrumentation amplifier (AD620), some passive components, operational amplifier (LM741), DAQ card, and laptop whereas Lab view is used as software. The software is used to exchange the data from analog to digital form, to perform the calculations, and to produce the ECG waveform on the monitor. Each of the processed in order to bring the signal in visible form and to limit the bandwidth of the signal. To do so, the instrumentation amplifier was used to amplify the tiny signal whereas passive and active components are used to design filter and to amplify it. Figure 4 illustrates the constructive circuit diagram of signal conditioning. The circuit has been designed and tested in multisim to get the appropriate output of signals.

Instrumentation Amplifier. The voltage gain of the instrumentation amplifier is calculated using the following equation:

$$A = 1 + \frac{49.4k\Omega}{1k\Omega}$$

components in this block diagram is explained in detail in the following subsections [4].

Surface Electrode. The principle of the electrode is to convert physical parameter into an electrical output. The

$$A = 1 + \frac{49.4k\Omega}{1k\Omega} = 1 + 49.4 = 50.4.$$

$$(1)$$

function of the transducer is to convert biological information into a quantifiable electrical signal. The transducer interface is provided using an electrode-electrolyte interface. The most preferable electrode is Ag/AgCl, as it reduces the impedance while using it and the gel is used for the proper contact between the surface of the skin and electrode.

Operational Amplifier. The voltage gain of the operational amplifier is estimated using given formula as the sedone is non-inverting amplifier:

$$\square = 1 + \frac{1}{2},$$

$$\underline{\square} = 1 + \frac{200k\Omega}{1k\Omega} = 1 + 200 = 201.$$

(2)

Signal Conditioning Circuit. After receiving an ECG signal from the subject through electrode, it has to be

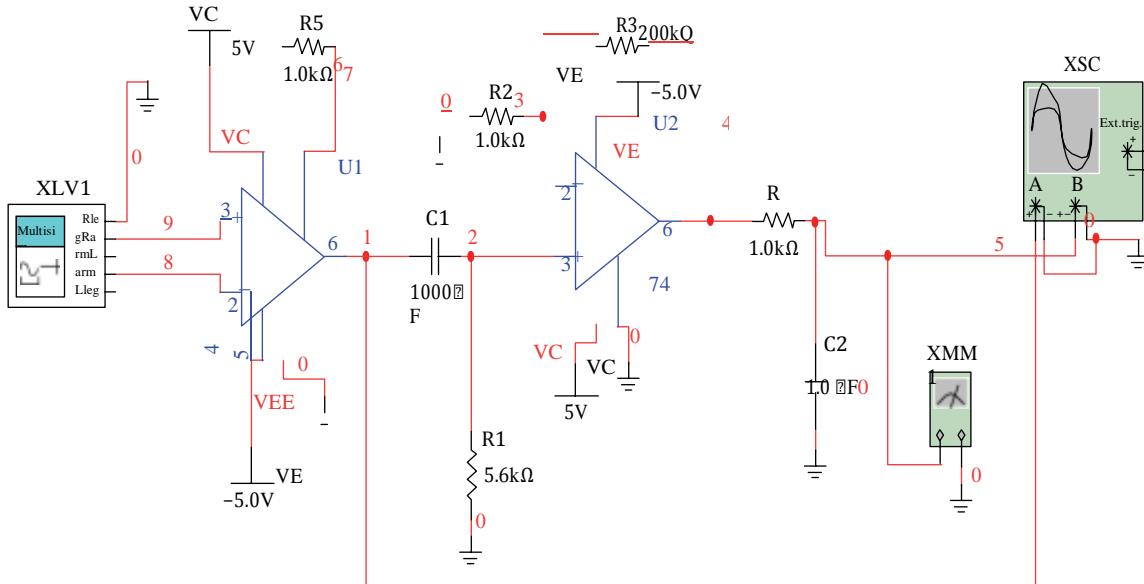


FIGURE 4: ECG signal acquisition and condition circuit.

High-Pass Filter. The output of the instrumentation amplifier is fed into the passive AC coupling with a cutoff frequency, $\omega_c = \frac{1}{R_1 C_1}$, of 0.02Hz such that high-pass filters

$$\underline{\square} = 1$$

$$\square_{\text{high-pass}} = 2^{\underline{\square}} \square_1 \square_1$$

1

and 12-bit analog-to-digital converter running at a sampling frequency up to 300 Hz, which can be increased up to 200KHz. This satisfies the sampling requirements of the ECG signal.

Laboratory Virtual Instrument Engineering Workbench (Labview). It is a graphically programmed computer language.

$$\underline{\square} = 2 * 3.14 * 5.6 * 10^3 * 1000 * 10^{-6}$$

(3)

guage for real-time instrumentation. It is a software package developed to build programs with symbols (icons) rather

$$\underline{\square} = 5$$

$$\square_{\text{high-pass}} = 3.14 * 56'$$

$$\square_{\text{high-pass}} = 0.02\text{Hz}$$

than writing out lines and lines of programming text. It uses symbols, terminology, and formats that are familiar to technicians, scientists, and engineers. Labview is programmed to act as an interface, helping pieces of hardware “communicate”

Low-Pass Filter. The second-stage amplified signal is fed into a low-pass filter with a cutoff frequency, $\omega_c = \frac{1}{R_3 C_2}$, of 160 Hz for removing high frequency noise or movement artifacts:

1

$$\square_{\text{low-pass}} = \frac{1}{2 * \pi * 4 * 2}$$

with each other. Moreover, Labview offers built-in libraries that allow the user to work over the Internet and use different programming formats and systems.

Simple Mail Transfer Protocol (SMTP). Figure 6 shows the step of SMTP of how the data is processed throughout the different stages and transferred to client. It is a part of the application layer of the TCP/IP protocol. Using a

$$= \frac{2 * 3.14 * 10 * 10^3 * 1 * 10^{-6}}{1000} \\ (4)$$

process called "store-and-forward," SMTP moves your

mail on and across networks. It works closely with something called the Mail Transfer Agent (MTA) to send your

$\square_{\text{low-pass}} =$
 $= 159.2 \text{ Hz.}$
 6.28
 communication to the right computer and e-mail inbox [<http://support.aycontrol.com/>].

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2.3.DAQCard(6008). The output of the signal condition in circuit should be sent to the NI DAQ card for the conversion of signal from analog to digital as it has the built-in analog-to-digital converter.

The given figure (Figure 5) gives the idea about the block diagram of NI USB-6008 which is a simple and low-cost multifunction I/O device from National Instruments [5]. It is used to digitize the amplified, filtered ECG signal. The NI USB-6008 card has 8 differential analog input channels

Designing Strategies

The approach that has been followed in the designing of device is included in Figure 7. There were several stages like finding the appropriate electrodes to acquire the signal from body of the subject and analog signal conditioning circuit includes filtering and amplifying stage, DAQ card, and digital signal processing and display system.

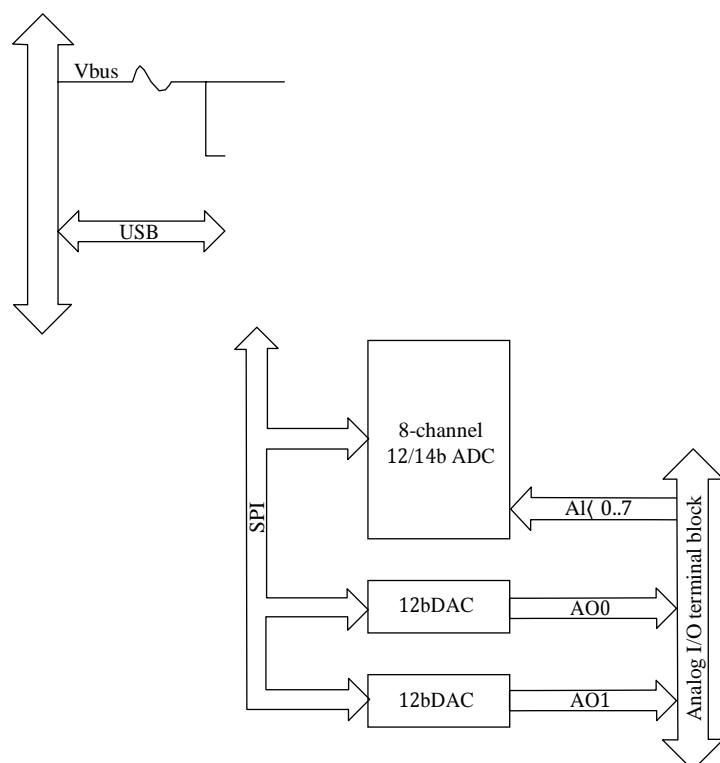


FIGURE 5: NI USB-6008 block diagram.

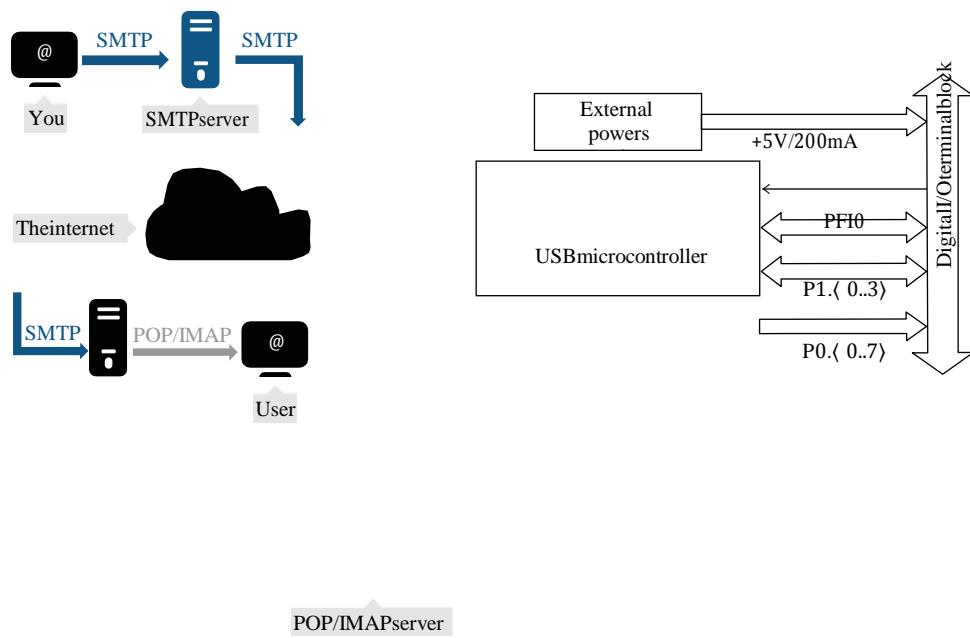


FIGURE6:SimpleMailTransferProtocol(refertohttp://www.serversmtp.com/en/free-smtp-server).

Designed Lab view Interface

The ECG system that has been developed is used for the continuous acquisition and chart recording of single input channels. It allowed users to record and save buffers of analog ECG data from one or more individuals, which is continuing.

Retrieving Input Signal. The analog signal is acquired from the breadboard and converted to the digital one through DAQ. Digital signal processing is done accurately as needed in order to produce high signal-to-noise ratio so that the heart diagnostics system is precise.

Digital Signal Processing. Here, the digital filters are done to remove the power line interferences and other artifacts available in the signal. The necessary data processing to display real-time ECG had been performed.

Threshold and Peak Detector. The threshold and peak indicators are implemented after processing. The purpose of these indicators is to provide some feedback to the user (i.e., physician) regarding the patient's average heart rate.

Figure 8 gives the idea about the complete ECG

system developed in Labview. The first part shows how the data have been acquired using data acquisition card (6008); in the next step, the retrieved data has been processed by BandPass Filter as well as notch filter to remove the heart artifacts from the signal [9,10]. Furthermore, the algorithm is developed to detect the peak of the signal.

The following given equation is used to calculate the heart rate and to identify the arrhythmia condition [11,12]:

$$60$$

– previously acquired into a circular buffer at the same time in that data previously retrieved from the buffer is plotted [6]

$$\text{HeartRate} = \frac{\Delta t}{T}$$

$$= \frac{\Delta t}{T} \quad (5)$$

8]. A common reason to read data while the acquisition is in progress is to process and display the data in virtual-realtime.

with Δt_1 being occurrence of first R wave and Δt_2 being occurrence of second R wave.

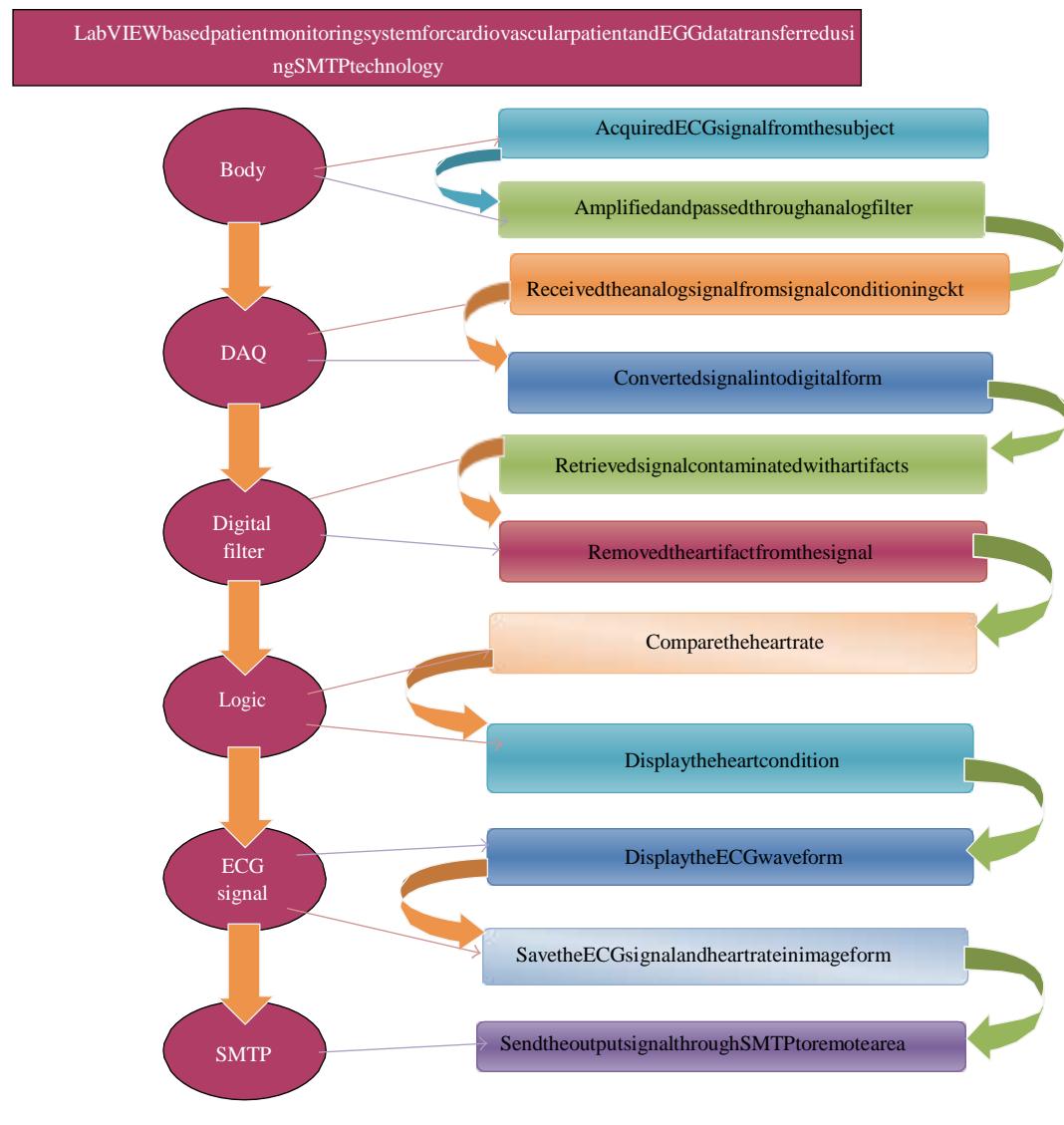


FIGURE 7: Designing strategy.

Dataacquisition Dataprocessing Datapresentation

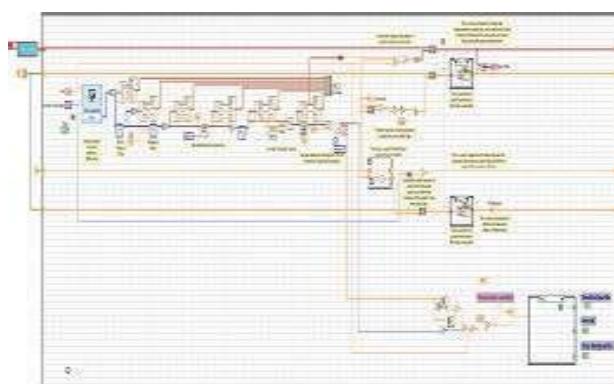


FIGURE8:Acquired,processed, andcalculatedheartrate.

DisplaySystemTool(Toshiba). After processing rawECGsignal, the signal has been displayed onto the laptop as shown in Figure 9. The display too is compatible with theprerequisiteoftheLabviewsoftware.

SMTP(SimpleMailTransferProtocol). Finally , the developed SMTP tool is used to send image file of acquired ECGsignal through Email Express VI, shown in Figure 10 that represents the front panel

and Figure 11 that represents the block panel developed using Labview which allows sending the data quickly through e-mails from Labview to a healthcare centre or physician.

II. RESULT

The given system is based on the principle of heart rate monitoring; it is able to produce the results shown in

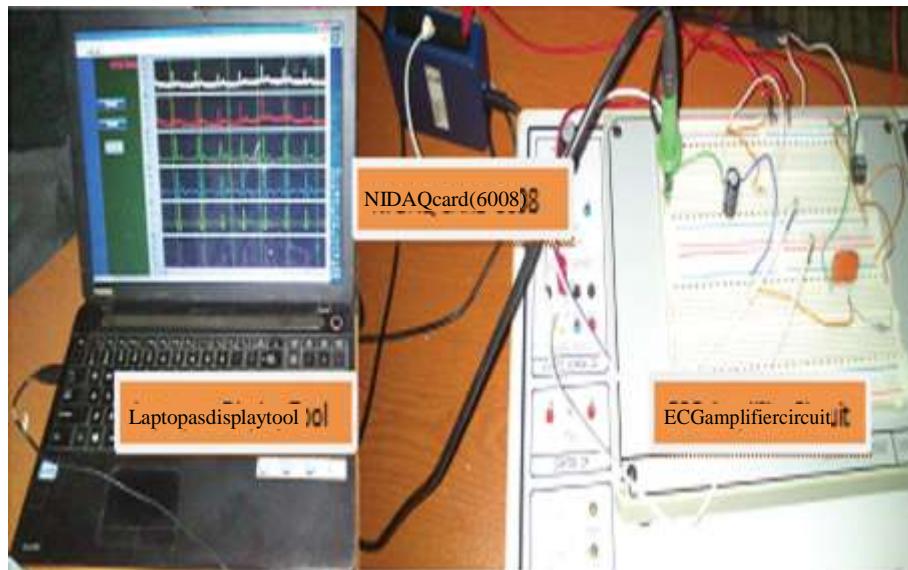


FIGURE9:ProposedECGdevice.

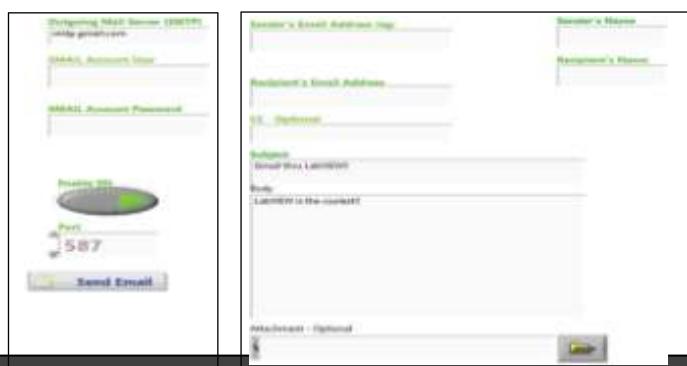


FIGURE10:FrontpanelofSMTP.

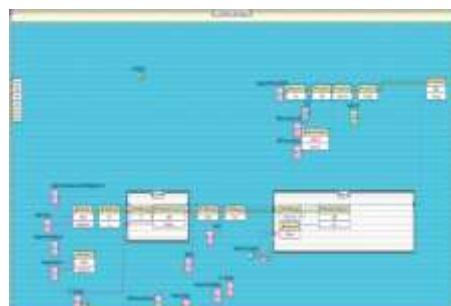


FIGURE11:BlockpanelofSMTP.

Figure12,whichshowaccurateECGsignalsandthecorrect calculation of both a resting and an elevated heart rate.Initially,therewasanissuewiththesystemregarding doctornotificationsubsystemwhichhasbeenshort by validatingtheproposed concept by running the VI at home, which sentbothtextandemailtoour“doctor”notifyingthemthattherewasadetected problemwiththe patient’s heart. It brings the freedom for the physician as well as for the doctor to checkup on patients hearts from time to time by seeing real-timewaveformsasshowninFigure12. The proposed device is functioning well once all thehardware connected properly to meet the criteria

for theproposedidea. Asawhole,it is very reliable andportable aswellascosteffective.

III. DISCUSSION

Mostoftheworkhasbeendonebasedeitheron hardwareoronsoftware. Inthecaseofhardware,totransmittheECG data, transmitter and receiver had been used, whichincreases the cost of the device, whereas the developed oneintegratedwithhardwarealongwithsoftwaretotransmitthe

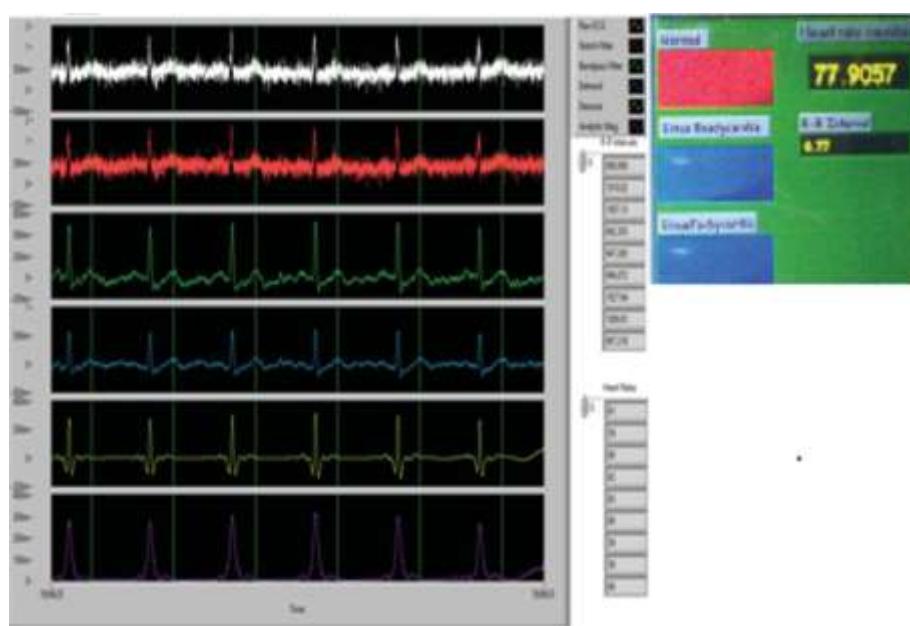


FIGURE12:Acquired,processedECGsignal.

data anywhere using SMTP technology. Thus, the completeddevicebecomesmoreuserfriendlyaswellascosteffective.

IV. CONCLUSION AND FUTUREWORK

In this paper, the low-cost biomedical measurement systemwiththeabilityofstorageindigitalformataswell

assendingthedataotheremoteareahasbeenpresented. Thehardwareimplementations using commercially available devices andthe software written in Labview program for continuouslymonitoring ECG

data have been described. The proposed measurement system is also capable of sending the data through SMTP to the physician or healthcare centre with no time. The proposed system could be modified by increasing the number of channels.

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